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(54) **BONE CUTTING GUIDE SYSTEMS AND METHODS**

(58) **Field of Classification Search**

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See application file for complete search history.

(71) Applicant: **Treace Medical Concepts, Inc.**, Ponte Vedra, FL (US)

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(72) Inventors: **Paul Dayton**, Fort Dodge, IA (US); **Robert D. Santrock**, Morgantown, WV (US); **Daniel J. Hatch**, Greeley, CO (US); **W. Bret Smith**, Lexington, SC (US); **Carlos Eduardo Gil**, Jacksonville Beach, FL (US); **Sean F. Scanlan**, Jacksonville, FL (US); **Joe William Ferguson**, Ponte Vedra Beach, FL (US); **F. Barry Bays**, Collierville, TN (US); **John T. Treace**, Ponte Vedra Beach, FL (US)

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(73) Assignee: **Treace Medical Concepts, Inc.**, Ponte Vedra, FL (US)

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(74) *Attorney, Agent, or Firm* — Fredrikson & Byron, P.A.

Related U.S. Application Data

(57) **ABSTRACT**

(63) Continuation of application No. 15/603,056, filed on May 23, 2017, which is a continuation of application No. 14/990,574, filed on Jan. 7, 2016, now Pat. No. 9,687,250.

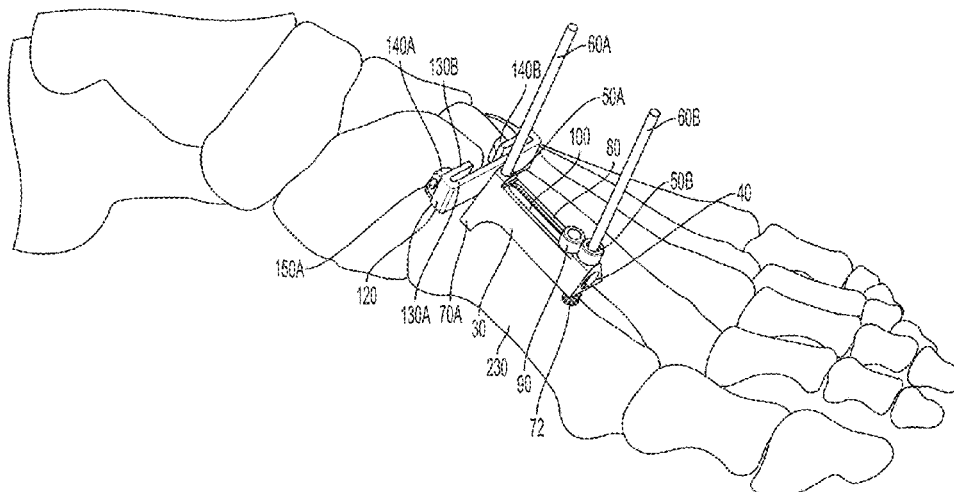
A bone cutting guide may include a support that contains a shaft movable relative to the support. The shaft may carry a guide member having one or more cut guides through which a clinician inserts a cutting member to cut bone positioned under the guide cut guides. In operation, a clinician may fixate the support of the bone cutting guide to a bone and translate the guide member until the one or more cut guides are positioned at a desired cut location. The clinician may then perform a cut through the cut guide. In some examples, the bone cutting guide includes additional components, such as bridging member or secondary cut guide, to provide additional functionality.

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20 Claims, 18 Drawing Sheets



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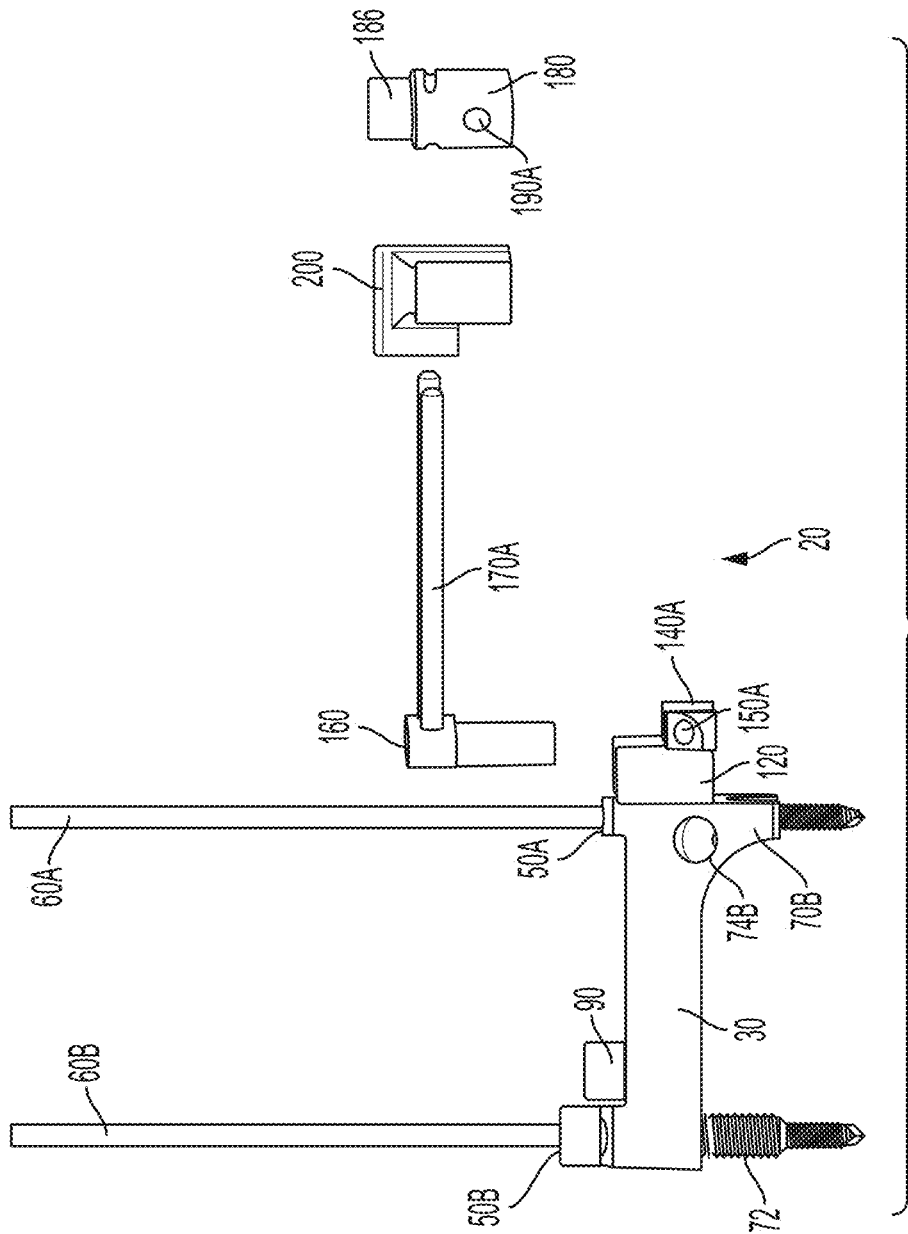


FIG. 1

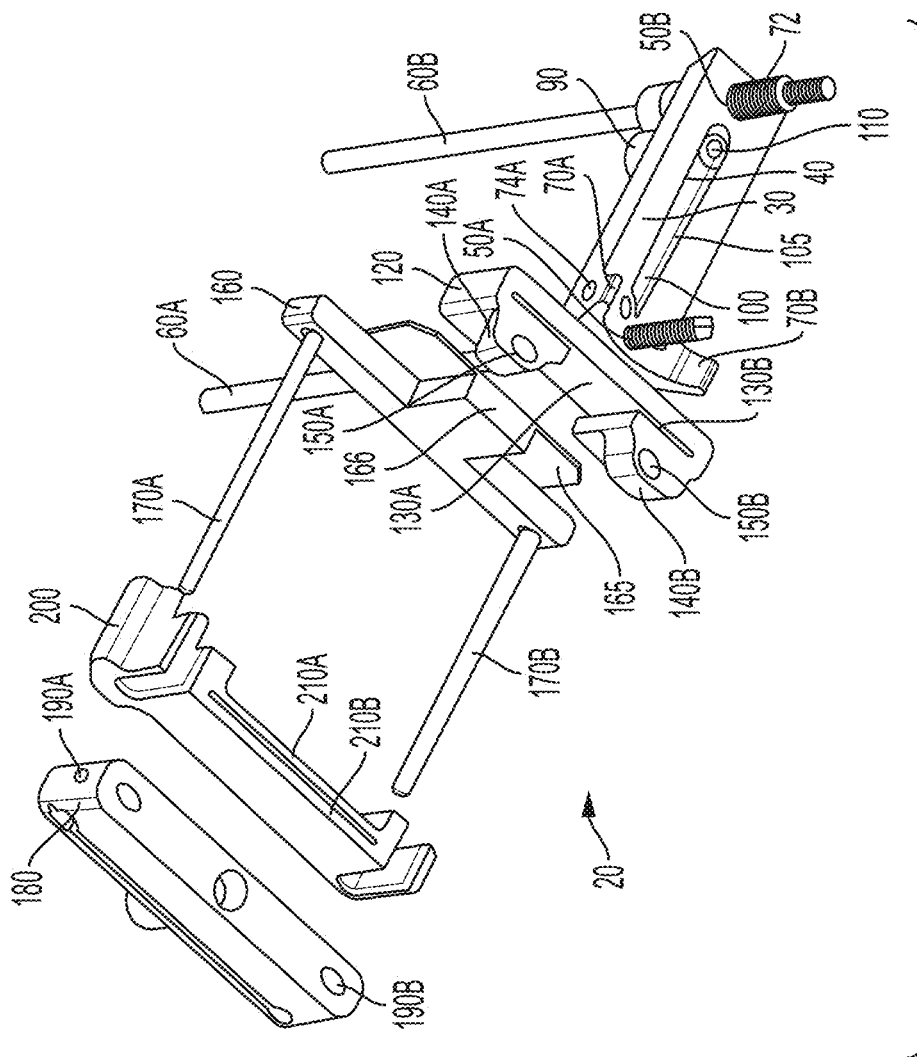


FIG. 2

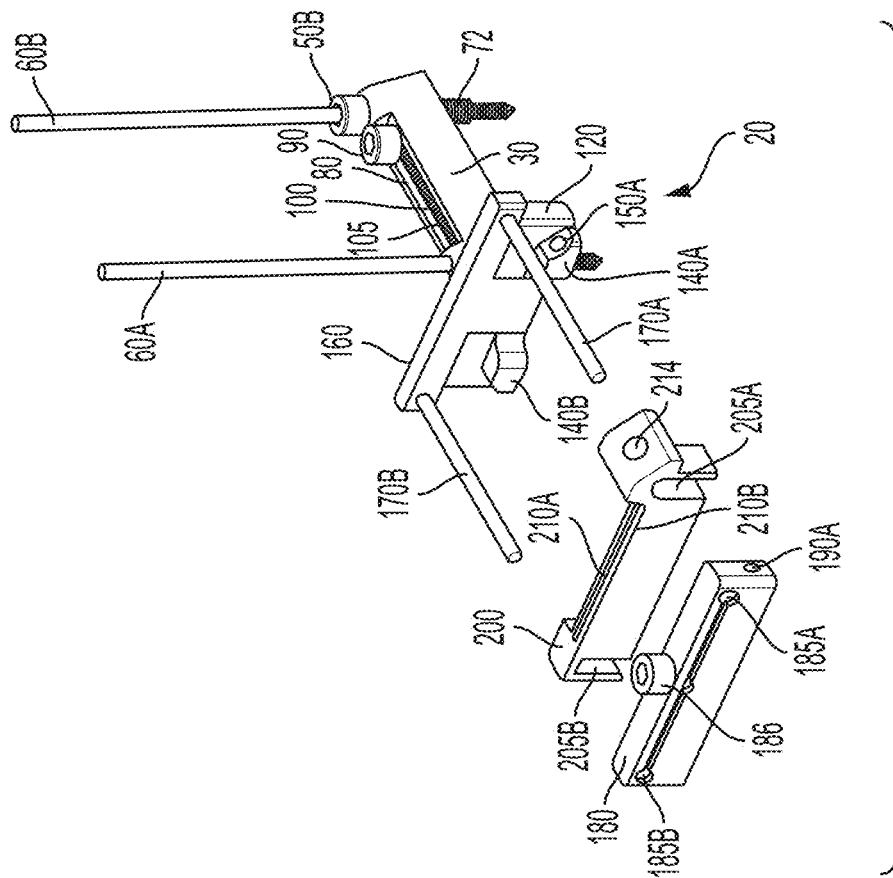


FIG. 3A

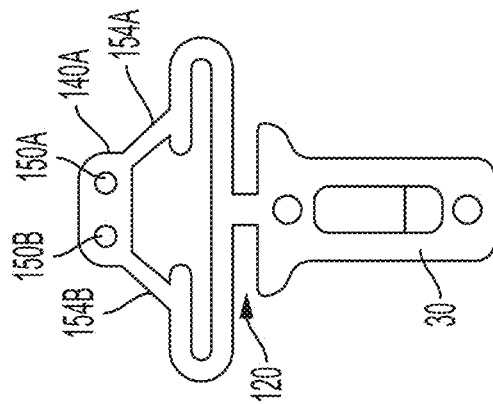


FIG. 3B

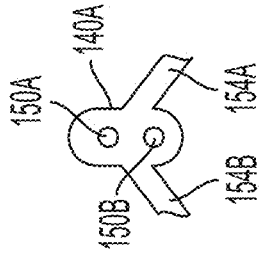


FIG. 3C

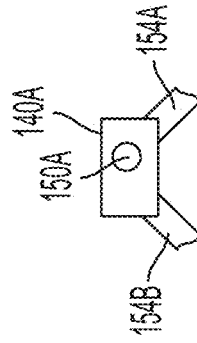


FIG. 3D

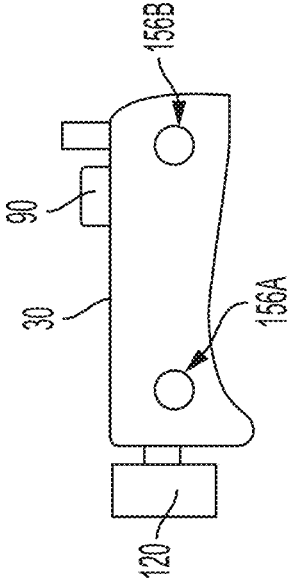


FIG. 3E

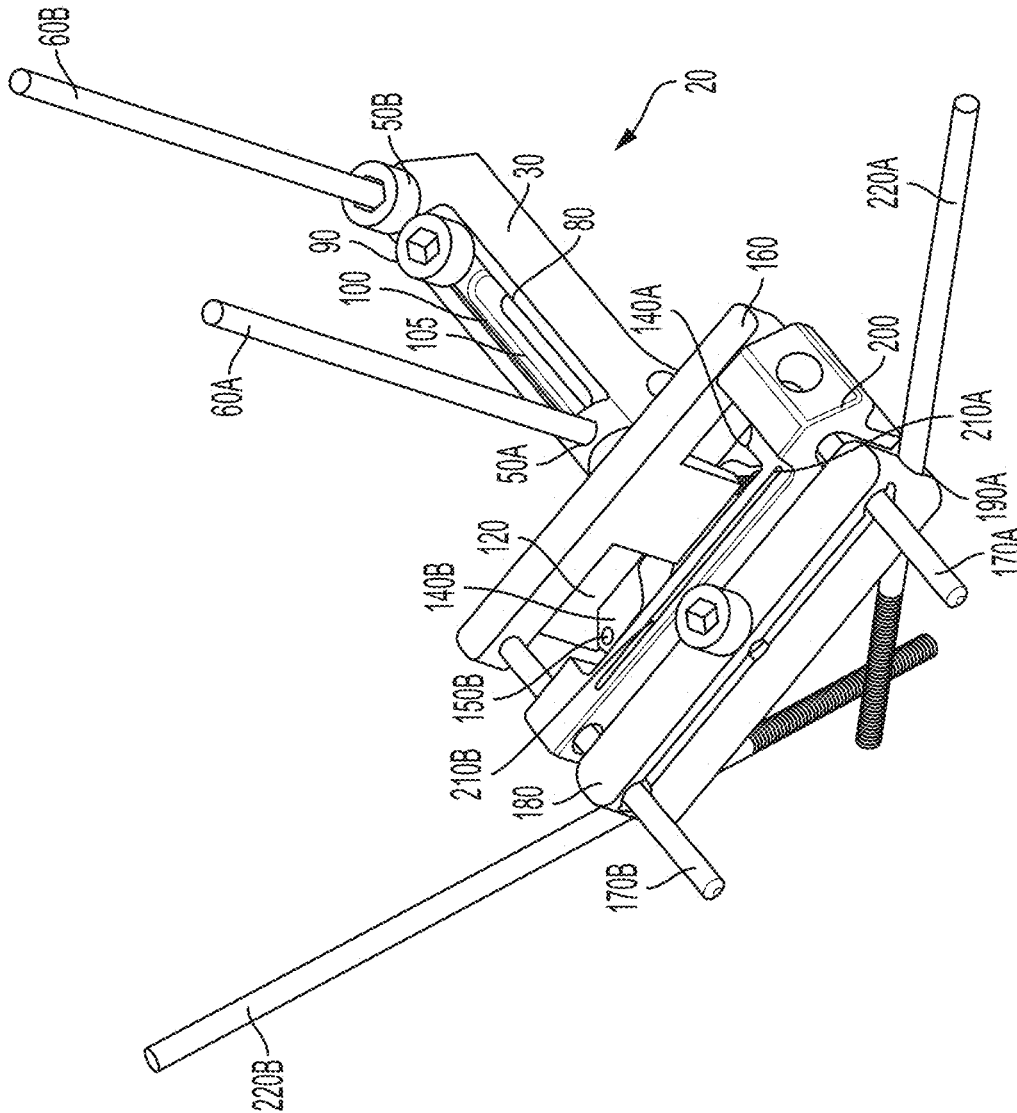


FIG. 4

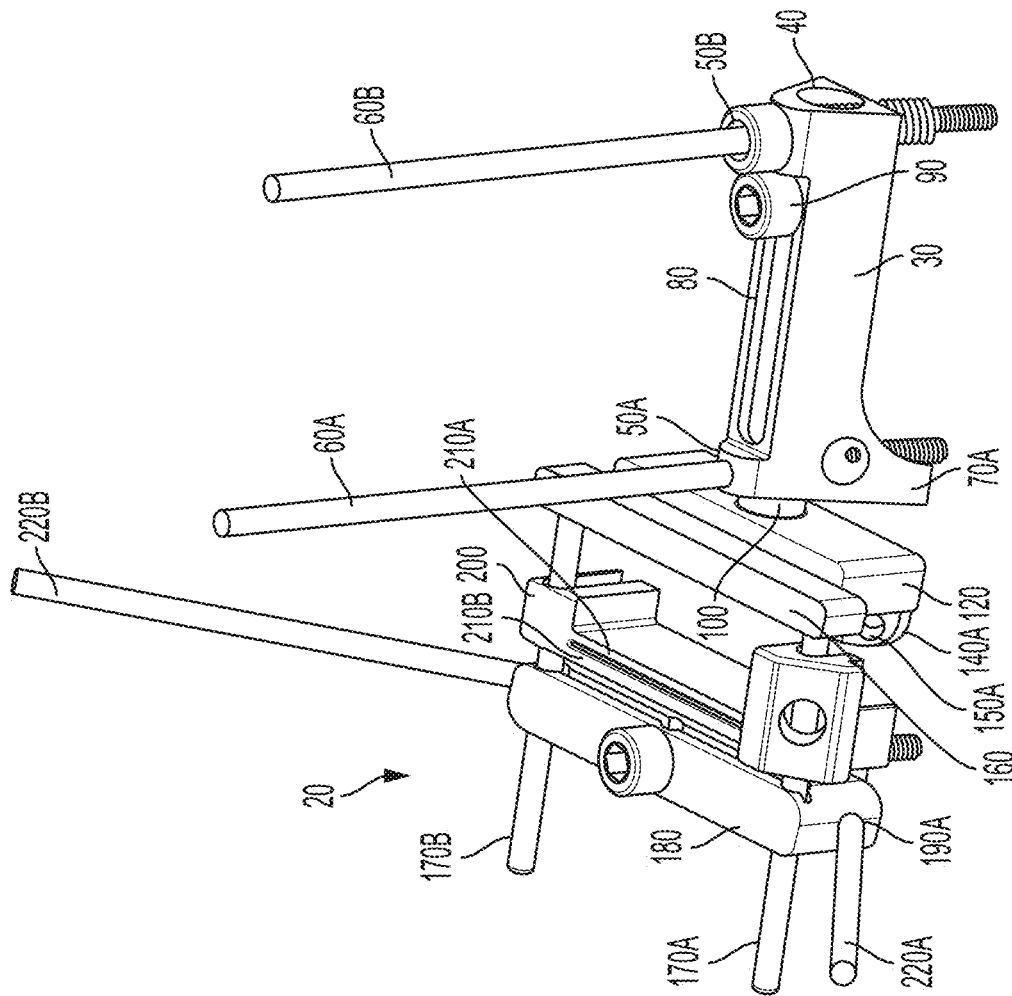


FIG. 5

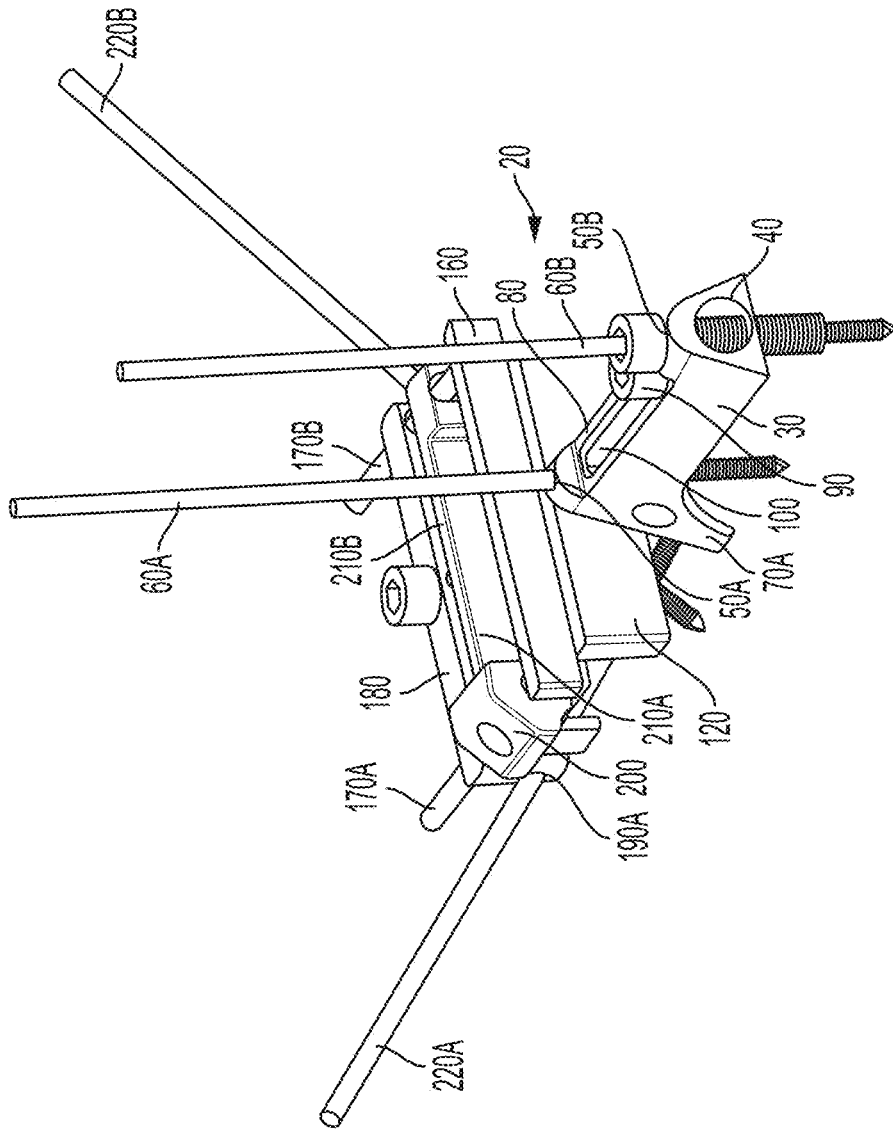


FIG. 6

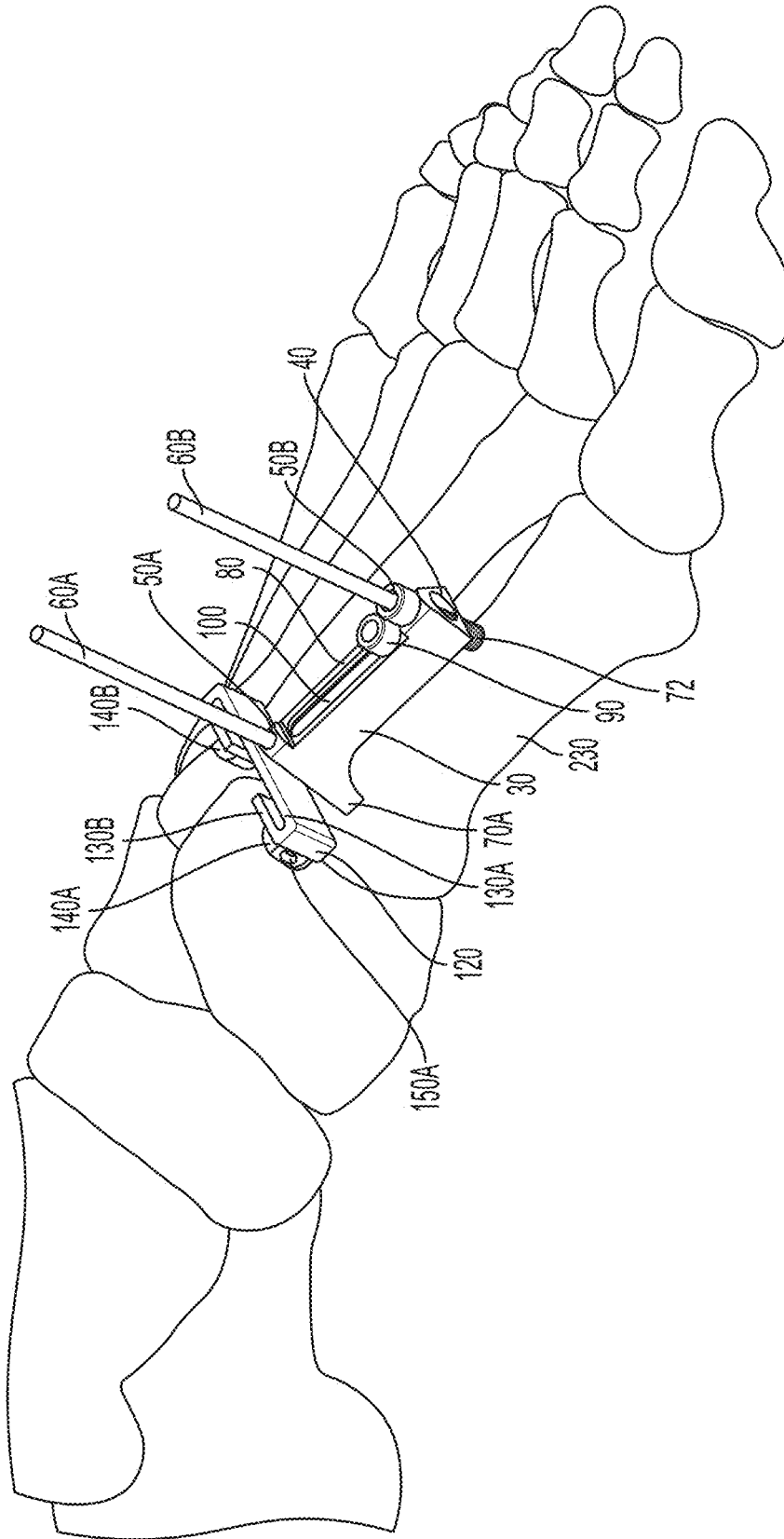


FIG. 7

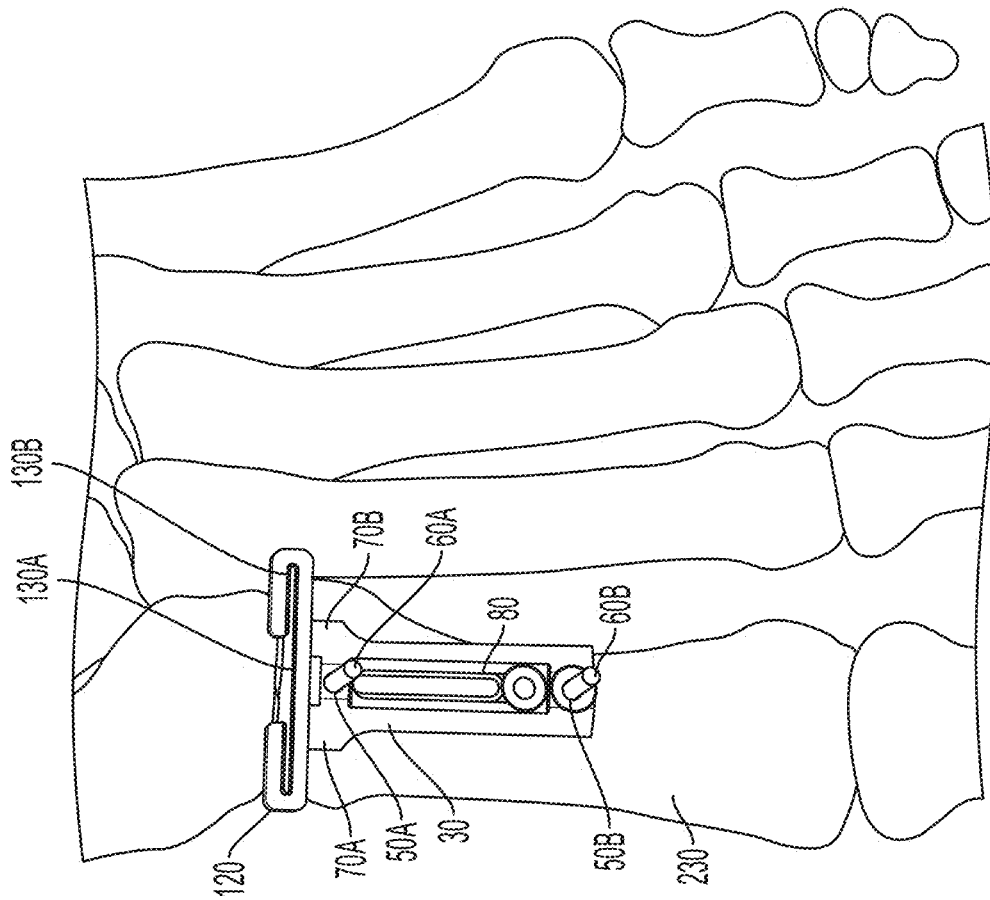


FIG. 8

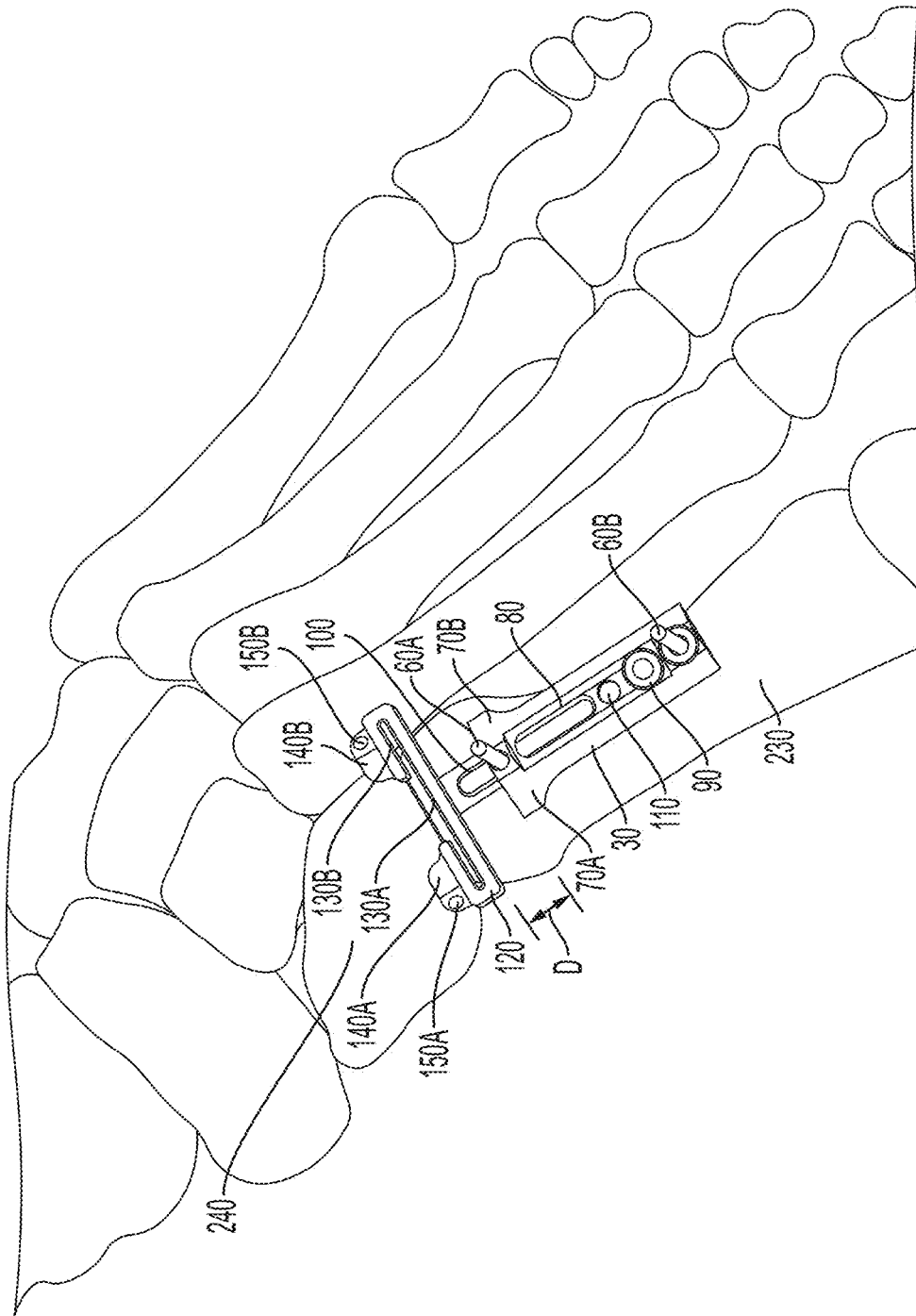


FIG. 9

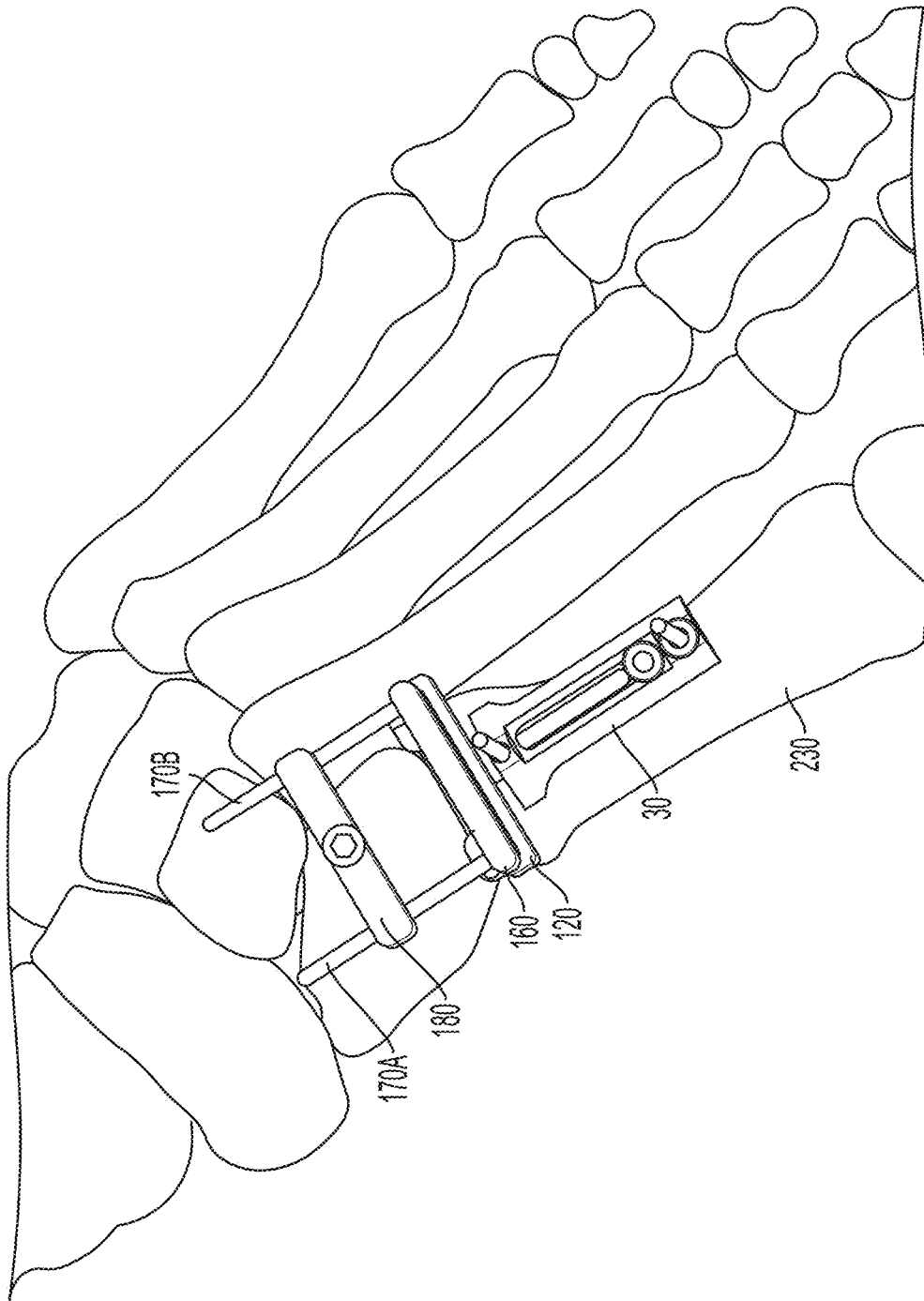


FIG. 10

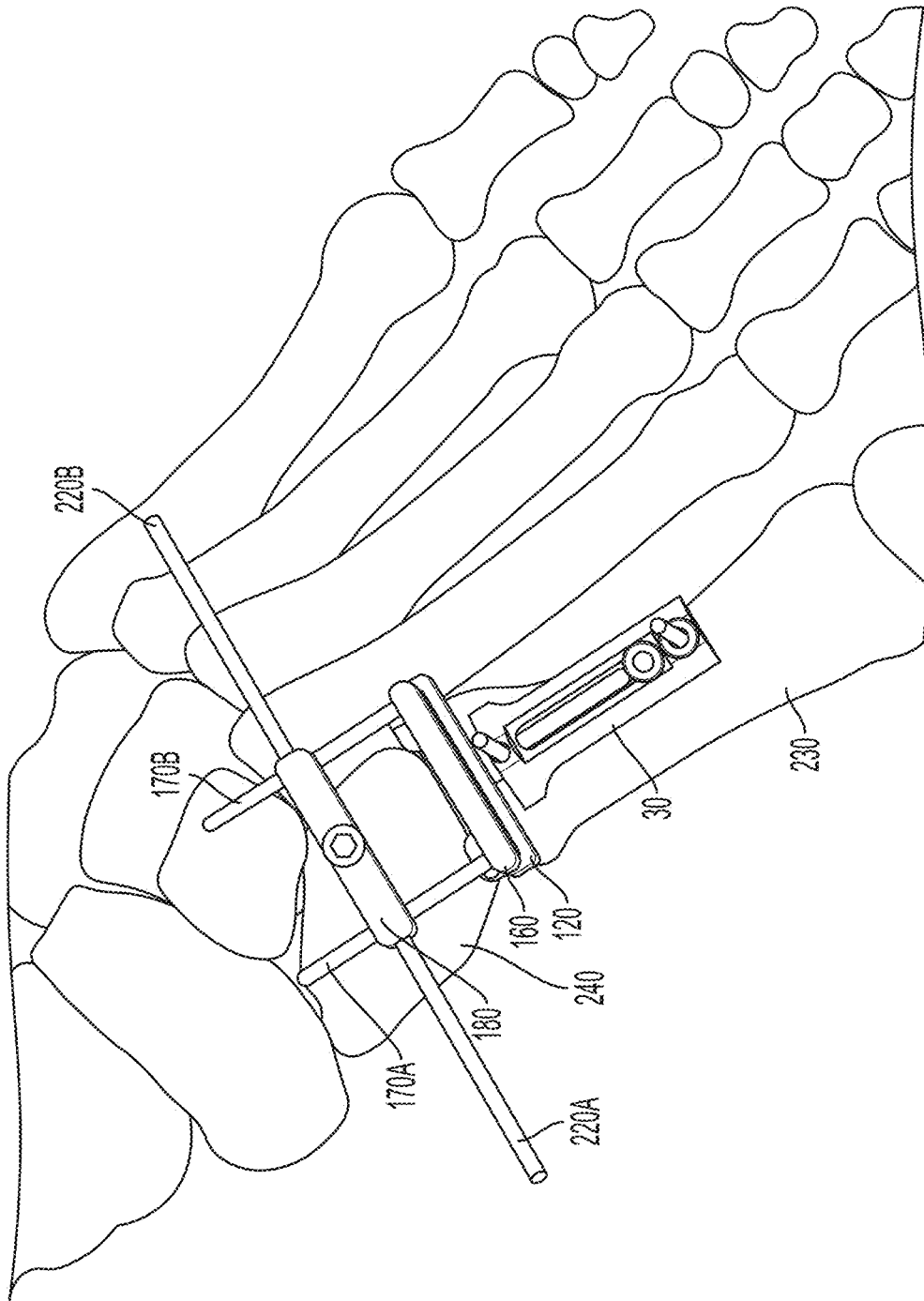


FIG. 11

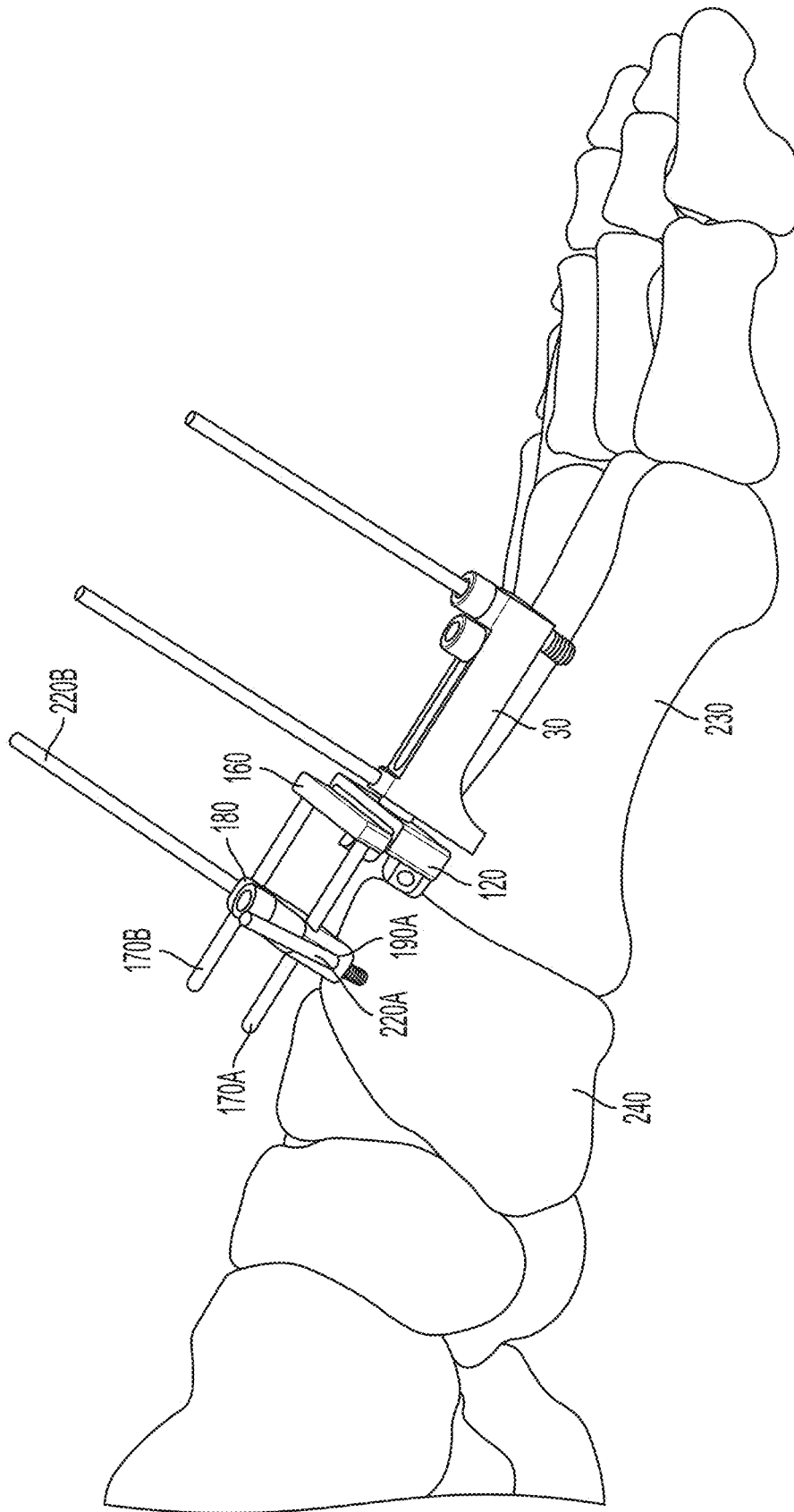


FIG. 12

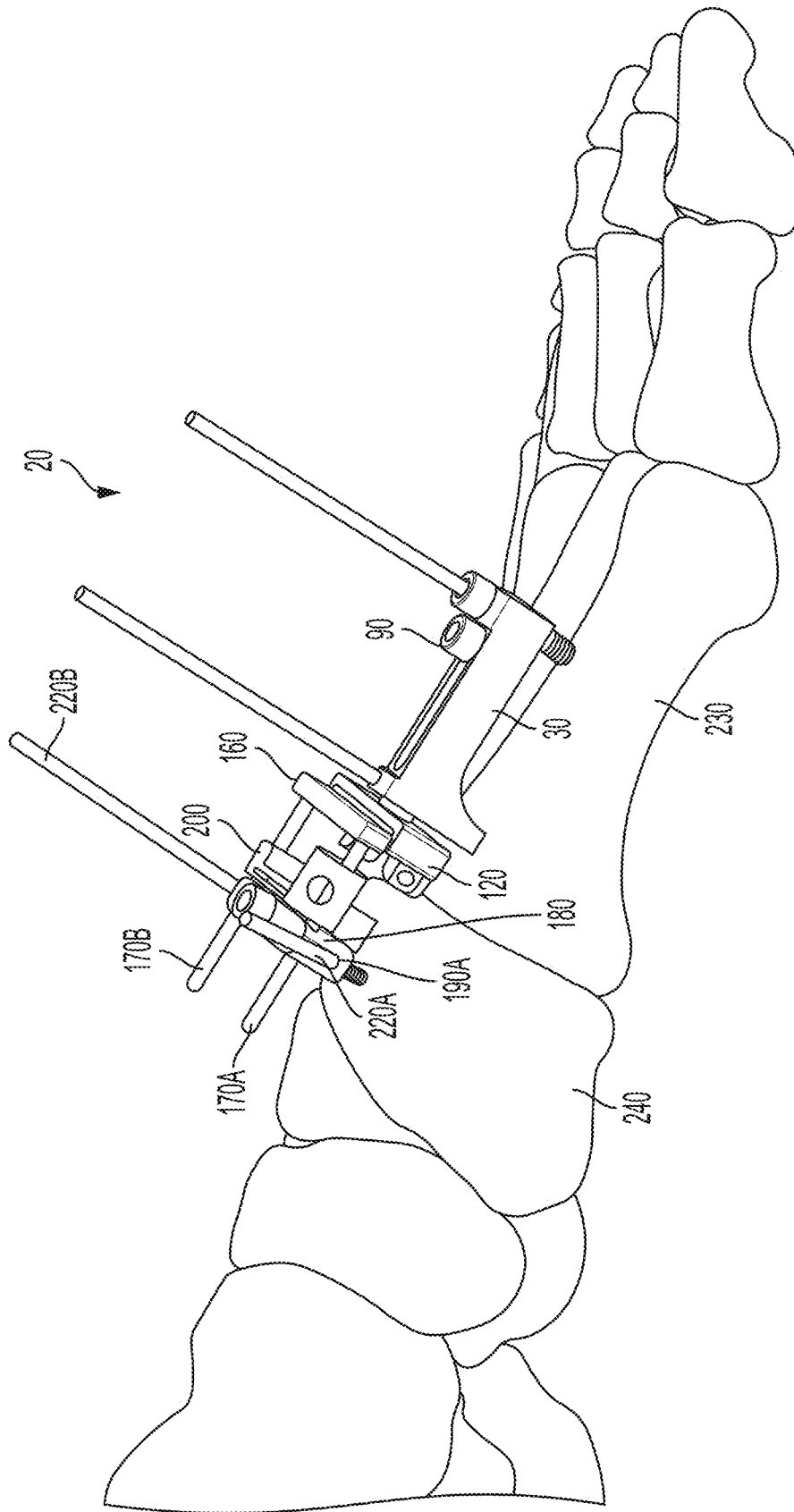


FIG. 14

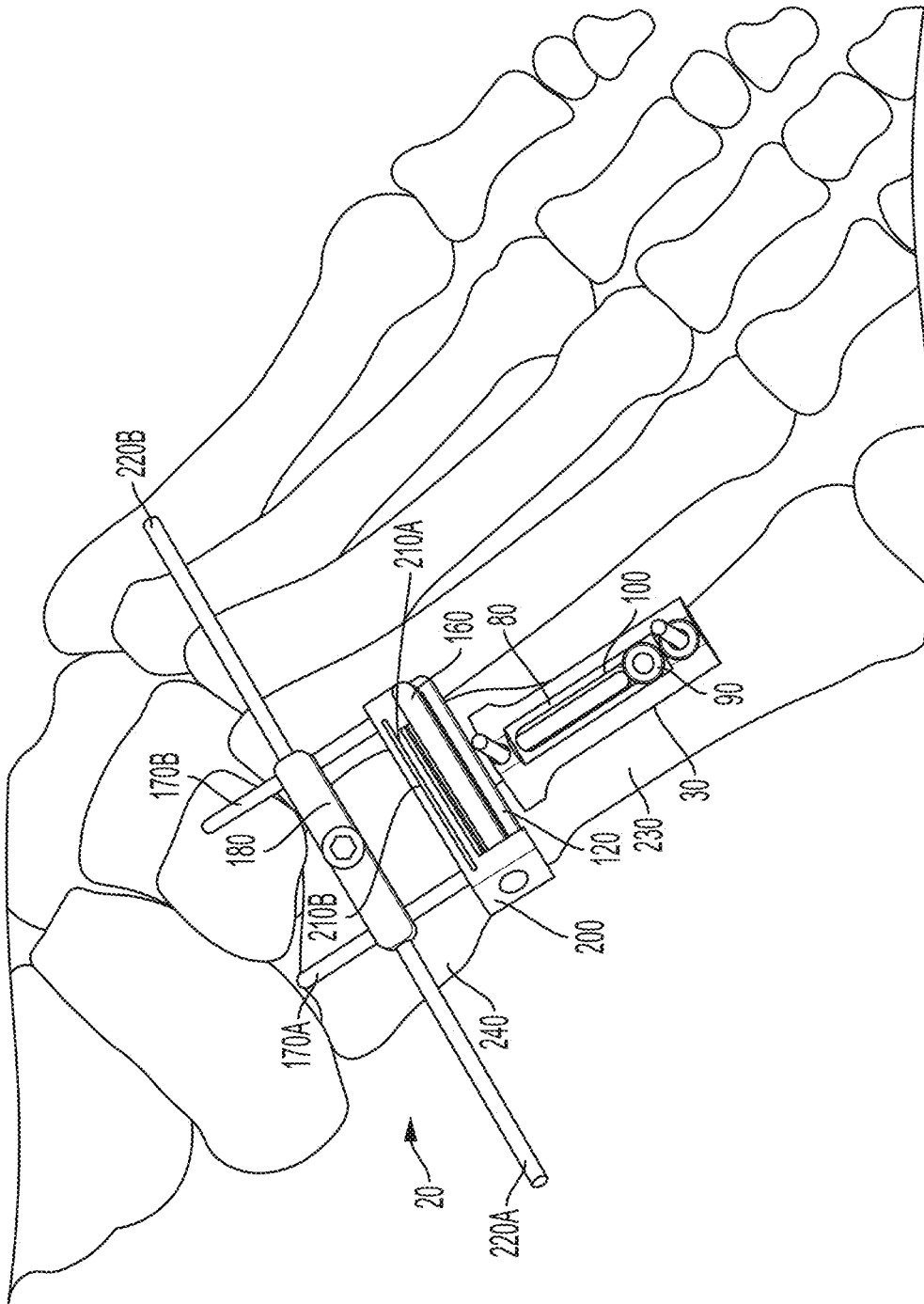


FIG. 15

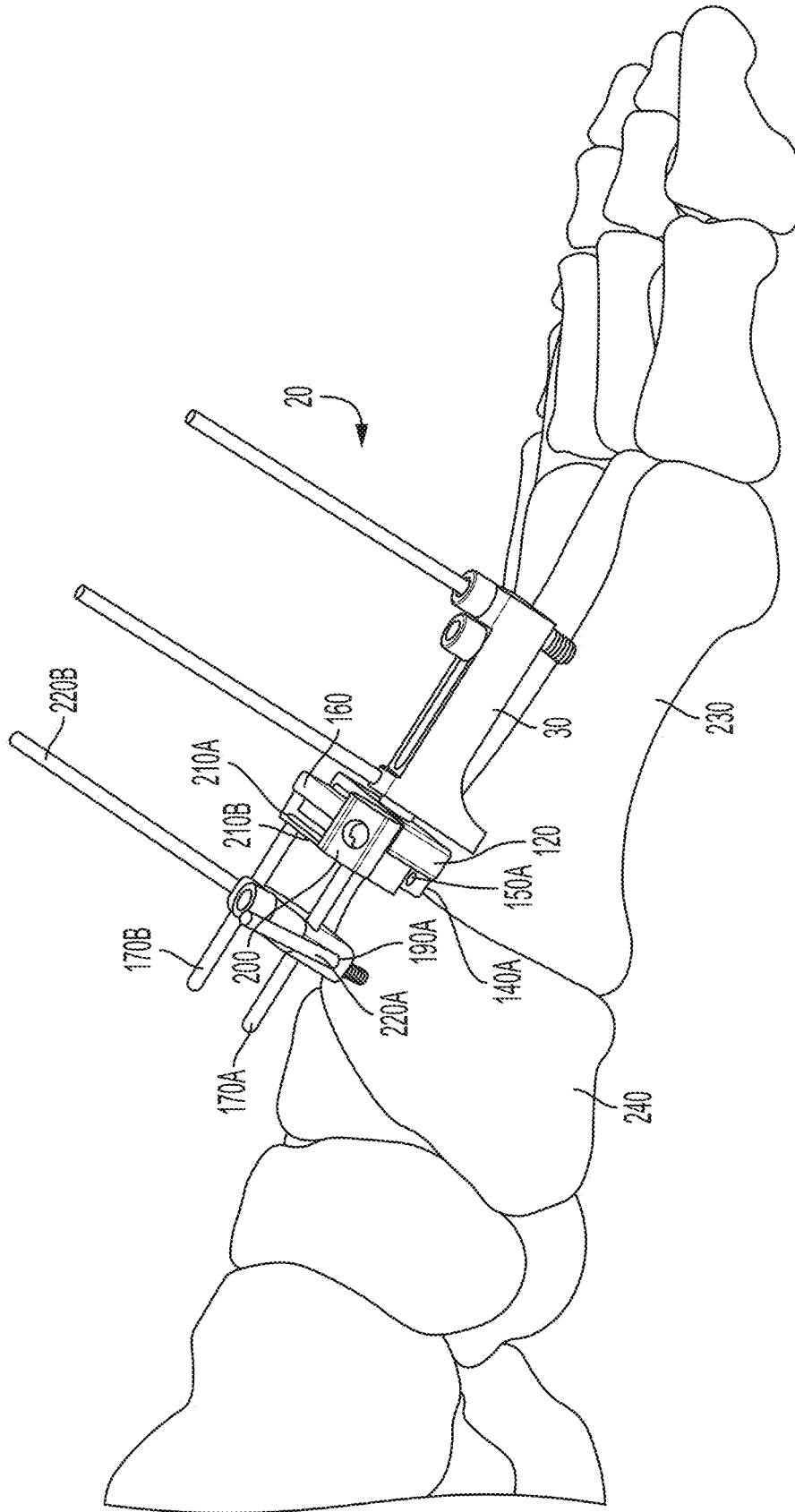


FIG. 16

BONE CUTTING GUIDE SYSTEMS AND METHODS

RELATED APPLICATION

This application is a continuation of U.S. patent application Ser. No. 15/603,056, filed May 23, 2017, which is a continuation of U.S. patent application Ser. No. 14/990,574, filed Jan. 7, 2016, and issued as U.S. Pat. No. 9,687,250 on Jun. 27, 2017, which in turn claims the benefit of U.S. Provisional Application Ser. No. 62/100,641, filed Jan. 7, 2015. The entire contents of each of these applications are hereby incorporated by reference.

TECHNICAL FIELD

This disclosure relates generally to devices and methods for positioning and cutting bones.

BACKGROUND

Bones, such as the bones of a foot, may be anatomically misaligned. In certain circumstances, surgical intervention is required to correctly align the bones to reduce patient discomfort and improve patient quality of life.

SUMMARY

In general, this disclosure is directed to bone cutting guide systems and techniques for cutting bones. In some examples, a bone cutting guide includes a main body, or support, that houses a shaft that can translate relative to the main body. The shaft may have a main guide member positioned on the end of the shaft. The main guide member may define opposed guide surfaces configured to receive a cutting member. For example, the cutting member may be inserted between the opposed guide surfaces and bounded within a range of movement by the guide surfaces, causing the cutting member to be directed at a cutting location under the guide surfaces. Additionally or alternatively, the main guide member may define a single cutting surface/plane. The cutting surface/plane may be a surface against which a clinician can position a cutting member and then guide the cutting member along the cutting surface/plane to perform a cutting operation.

The main body of the bone cutting guide can include fixation members, such as fixation pins or apertures, that allow the main body to be fixated on or adjacent a bone to be cut. For example, in use, a clinician may fixate the main body to a bone (e.g., a first metatarsal). Thereafter, the clinician may translate the main guide member having at least one cutting guide surface (e.g., opposed cutting guide surfaces) relative to the fixed main body. The clinician can translate the main guide member by sliding or rotating the shaft housed within the main body, e.g., causing the distal end of the shaft and main guide member carried thereon away from or towards the main body. Once suitably positioned, the clinician may or may not lock the location of the shaft and perform one or more cuts through the guide surfaces of the main guide member.

In some configurations, the bone cutting guide also includes a bridge component that can form a bridge over a section of bone, such as a joint between adjacent bones (e.g., first metatarsal-medial cuneiform joint). For example, the bridge component may have a proximal end that is attachable to the main guide member carried on the shaft attached to the main body and a distal end separated by one or more

rails. The proximal end may be insertable between the opposed cutting guide surfaces of the main guide member, e.g., such that the proximal end of the bridge can be inserted between the guide surfaces after performing a cut through the guide surfaces. The distal end of the bridging member can include fixation members, such as fixation pins or apertures, that allow the distal end of the bridging member to be fixated to bone. In one application, the distal end of the bridging member is fixated to a different bone than the bone the main body is fixated to such that the bridging member spans a joint. In such applications, joint spacing may be expanded or contracted by translating the shaft carried by the main body.

In addition to or in lieu of providing a bridging member, in some additional configurations, the bone cutting guide may include a secondary guide member. The secondary guide member can be positioned distally of the main guide member and may also include guide surfaces, such as opposed guide surfaces forming a channel sized and shaped to receive a cutting member. The secondary guide member may facilitate making a second bone cut distal of a location where a first bone cut is made using the main guide member.

In one example, a bone cutting guide is described that includes a support defining an inner cavity and a shaft disposed at least partially within the inner cavity, where the shaft is translatable within the inner cavity relative to the support. The bone cutting guide also includes a main guide member located on an end of the shaft, where the main guide member includes a first guide surface defining a first plane and a second guide surface defining a second plane, and where the first plane is parallel to the second plane.

In another example, a method for cutting bones is described. The method includes fixing a support to a bone and aligning a main guide member to be positioned at a location to be cut. The method further includes making a first cut at the location to be cut by inserting a cutting member through a space defined between a first guide surface of the main guide member and a second guide surface of the main guide member.

The details of one or more examples are set forth in the accompanying drawings and the description below. Other features, objects, and advantages will be apparent from the description and drawings, and from the claims.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a side view of an embodiment of a bone cutting guide, with some components shown in an exploded view.

FIG. 2 is a perspective view of the bone cutting guide of FIG. 1.

FIG. 3A is a perspective view of the bone cutting guide of FIG. 1 with a bridge component attached to a main guide member.

FIGS. 3B-3D are top plan view illustrations of a bone cutting guide with different example connecting blocks.

FIG. 3E is a side plan view of a bone cutting guide and an exemplary support.

FIG. 4 is a perspective view of the bone cutting guide of FIG. 1 assembled.

FIG. 5 is another perspective view of the bone cutting guide of FIG. 4.

FIG. 6 is a further perspective view of the bone cutting guide of FIG. 4.

FIG. 7 is a perspective view of a bone cutting guide support fixed to a bone.

FIG. 8 is a top view of the bone cutting guide support fixed to the bone of FIG. 7.

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FIG. 9 is a perspective view of the bone cutting guide support fixed to the bone of FIG. 7 with a location of the main guide member adjusted.

FIG. 10 is a perspective view of a bridge component attached to the main guide member of the support of FIG. 7 with a fixation structure attached to the bridge component.

FIG. 11 is a perspective view of the fixation structure pinned across a bone.

FIG. 12 is another perspective view of the pinned fixation structure of FIG. 11.

FIG. 13 is a perspective view of the assembled bone cutting guide fixed to bones.

FIG. 14 is a further perspective view of the assembled bone cutting guide of FIG. 13.

FIG. 15 shows a perspective view of the assembled bone cutting guide of FIG. 13 with a secondary guide member translated along rails of the bridge component.

FIG. 16 is an additional perspective view of the assembled bone cutting guide of FIG. 15.

DETAILED DESCRIPTION

The following detailed description is exemplary in nature and is not intended to limit the scope, applicability, or configuration of the invention in any way. Rather, the following description provides some practical illustrations for implementing exemplary embodiments of the present invention. Examples of constructions, materials, and dimensions are provided for selected elements, and all other elements employ that which is known to those of ordinary skill in the field of the invention. Those skilled in the art will recognize that many of the noted examples have a variety of suitable alternatives.

Embodiments of the present invention include a bone cutting guide. In an exemplary application, the bone cutting guide can be useful during a surgical procedure, such as a bone alignment, osteotomy, fusion procedure, and/or other procedures where one or more bones are to be cut. Such a procedure can be performed, for example, on bones (e.g., adjacent bones separated by a joint or different portions of a single bone) in the foot or hand, where bones are relatively smaller compared to bones in other parts of the human anatomy. In one example, a procedure utilizing the bone cutting guide can be performed to correct an alignment between a metatarsal (e.g. a first metatarsal) and a cuneiform (e.g., a first cuneiform), such as a bunion correction. An example of such a procedure is a lapidus procedure. In another example, the procedure can be performed by modifying an alignment of a metatarsal (e.g. a first metatarsal). An example of such a procedure is a basilar metatarsal osteotomy procedure.

FIGS. 1, 2, and 3A show an embodiment of a bone cutting guide 20 with some components of the bone cutting guide 20 shown in an exploded view. FIG. 1 is a side view of the bone cutting guide 20, while FIGS. 2 and 3A are perspective views of the bone cutting guide 20. The bone cutting guide 20 can include a support 30 which defines an inner cavity 40 (FIG. 2). In one embodiment, the support 30 can include a first fixation aperture 50A and a second fixation aperture 50B, each of which can extend through the support 30 and receive fixation pins 60A and 60B, respectively, such that the fixation pins 60A and 60B extend through the support 30 via the fixation apertures 50A and 50B. In the embodiment shown, the fixation pins 60A and 60B have a threaded first end adapted to threadingly engage with a bone, and allow the support 30 to be translated along a longitudinal axis of both pins 60A and 60B. In the illustrated embodiments, the

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fixation apertures 50A and 50B are located on opposite longitudinal ends of the support 30, but in other embodiments the fixation apertures 50A and 50B can be located at various positions on the support 30.

The support 30 can further include one or more extensions 70A and/or 70B protruding generally radially out from the support 30, which may define a concave surface configured to receive a generally cylindrical bone portion. In the embodiment shown, fixation aperture 50B is provided with an extension member 72 which can be threadingly coupled to the support 30. Such an extension member 72 can be adjusted relative to the support 30 to allow the support to become parallel with a longitudinal axis of a bone, if desired. In such embodiments, the support 30 can rest on a bone via the extensions 70 AB and extension member 72 in a position generally parallel to the bone. Fixation pin 60B may be received within an internal aperture of the extension member 72. As shown, apertures 74A and B, such as tapered apertures, may be provided proximal to extensions 70 A and B. Such apertures may extend through the support at a skewed angle relative to the longitudinal axis of the support, and may be used to engage a clamping instrument or receive fixation pins.

The support 30 can also include a slot 80 formed on at least a portion of a surface of the support 30. As illustrated in the embodiment of the cutting guide 20 shown in FIG. 3A, the slot 80 can extend in a surface of the support 30 between fixation apertures 50A and 50B. A securing component 90 can be configured to translate along the slot 80 relative to the support 30. For example, the securing component 90 can have a first end with a diameter greater than a diameter of a second opposite end, such that the first end of the securing component 90 is supported by the slot 80 (e.g., the first end has a diameter greater than a radial width of the slot 80) while the second end of the securing component 90 is positioned within the slot 80 (e.g., the second end has a diameter less than a radial width of the slot 80).

The inner cavity 40 of the support 30 can have a shaft 100 positioned at least partially within the inner cavity 40. The shaft 100 can be configured to translate within the inner cavity 40 relative to the support 30, such that an end of the shaft 100 can be made to project out from the inner cavity 40. The shaft 100 may define a slot 105 which may be aligned with the slot 80 defined by the support 30. This slot 105 may receive the pin 60A to reduce interference when the shaft 100 translates. Furthermore, the shaft 100 can include a securing aperture 110 which can be configured to receive at least a portion of the securing component 90. In one embodiment, both the second end of the securing component 90, within the slot 80, and the securing aperture 110 can be threaded to allow the securing component 90 to mate with the securing aperture 110. Such a configuration can allow the shaft 100 to be fixed, such as by compressing a surface of the support 30 that defines the slot 80, and thus prevented from translating within the inner cavity 40, relative to the support 30. In another embodiment, the securing component 90 can be threadingly engaged with the support 30 to act against the shaft 100 to prevent the shaft 100 from traveling with the cavity 40 when desired.

On an end of the shaft 100, a main guide member 120 can be disposed. In some embodiments the main guide member 120 can be integral with the shaft 100, or in other embodiments the main guide member 120 and the shaft 100 can be separate components coupled together. The main guide member 120 can have a first guide surface 130A and a second guide surface 130B, and in some embodiments the main guide member 120 can include blocks 140A and/or

140B. The first and second guide surfaces **130A** and **130B** can be adjacent surfaces facing one another with a space defined between the first and second guide surfaces **130A** and **130B**. For example, the first guide surface **130A** can be a surface of the main guide member **120** immediately opposite a surface of the main guide member **120** that interfaces with the shaft **100**, and the second guide surface **130B** can be a surface of the main guide member **120** immediately opposite a surface of the main guide member **120** that includes blocks **140A** and **140B**.

In the illustrated embodiment, the second guide surface **130B** contains a gap, such that the second guide surface **130B** is not a single, continuous surface. In other embodiments, the second guide surface **130B** can be a single, continuous surface lacking any such gap. The first guide surface **130A** defines a first plane, while the second guide surface **130B** defines a second plane. As shown, the first guide surface **130A** and the second guide surface **130B** can be configured such that the first plane is parallel to the second plane, with the space between. In further embodiments (not illustrated), the guide surfaces **130A** and **130B** can be configured such that the first and/or second planes are skewed.

As previously noted, a surface of the main guide member **120** can include one or more blocks **140A** and **140B**, either integral with the main guide member **120** or as separate components attached to the main guide member **120**. As shown, the blocks **140A** and **140B** can be on a surface on a side of the main guide member **120** furthest from the interface with the shaft **100**. In other applications, the blocks **140A** and **140B** can be located at various other positions on the main guide member **120**. The blocks **140A** and **140B** can include fixation apertures **150A** and **150B** respectively. The fixation apertures **150A** and **150B** extend through the blocks **140A** and **140B** and provide a location for configuring additional fixation pins to, for example, position a bone or bones.

As shown in FIGS. 3B-3D, the main guide member **120** and at least one block **140A** can assume other configurations. In FIG. 3B, the block **140A** includes fixation apertures **150A** and **B** and is spaced from the guide surfaces a distance via connecting flanges **154A** and **154B**. In the embodiment of FIG. 3B, the fixation apertures **150A** and **B** are positioned in a line substantially parallel to the guide surfaces. In FIG. 3C, the orientation of the fixation apertures **150A** and **B** is substantially perpendicular to the guide surfaces. In FIG. 3D, only one fixation aperture **150A** is provided.

Another embodiment of a support **30** is depicted in FIG. 3E. In FIG. 3E, the support **30** has at least one (e.g., two) fixation aperture **156A** and **156B** formed in its side to receive fixation pins. Such apertures can also be included on the opposite side of the support (not shown). In some embodiments, the fixation apertures **156A** and **156B** can be positioned in a line substantially parallel with a longitudinal axis of the support, and can extend in a direction substantially perpendicular to the longitudinal axis of the support. In certain embodiments, the apertures extend at an angle, such as about 20 degrees, from vertical. In such embodiments, the support **30** can be placed on a dorsal surface and after a first cut or cuts, can be rotated about a pin extending through one of the fixation apertures **156A** and **156B** to rotate the support relative to the bone and first cut or cuts. The support can then be further pinned to the bone and an additional cut or cuts can be made at a desired angle relative to the first cut or cuts.

In addition to the support **30**, the bone cutting guide **20** can include a bridge component **160**. As shown in FIG. 3A, the bridge component **160** can attach to the main guide

member **120**. In particular, in some applications of the bone cutting guide **20**, the bridge component **160** can have a geometry that allows the bridge component **160** to attach to the main guide member **120** between the first and second guide surfaces **130A** and **130B** through an interference fit. Optionally, a locking mechanism can be provided to lock the bridge component to the main guide member, such as a locking tab, screw, pin, cam, etc. For example, the bridge component **160** may have a planar member **165** (shown in FIG. 2) that is received within the gap between the surfaces **130A** and **130B** and an extending block **166** (shown in FIG. 2) adapted to extend into the surface gap of **130B**. In other applications, the bridge component **160** can be coupled to the main guide member **120** by any attachment mechanism, such as screws or clamps. The bridge component **160** can include rails **170A** and **170B**, each extending out from the bridge component **160** in a same general direction. In other embodiments, the rails **170A** and **170B** can extend out from the bridge component **160** at different angles.

The bone cutting guide **20** can also include in some embodiments a fixating structure **180**. The fixating structure **180** can be supported on the rails **170A** and **170B**. For example, the fixating structure **180** can include apertures **185A** and **185B** to receive the rails **170A** and **170B**, respectively. The fixating structure **180** can be secured to the rails **170A** and **170B**, such that the fixating structure **180** is obstructed from translating along the rails **170A** and **170B**, by turning or otherwise actuating an actuator **186** of the fixating structure **180**, which moves a lock (not shown) to act against the rails. Furthermore, the fixating structure **180** can also include one or more fixation apertures **190A** and/or **190B**. Fixation apertures **190A** and **190B** extend through fixating structure **180** and can be located on opposite ends of the fixating structure **180**, at a skewed angle, and serve to receive fixation pins or other means for stabilizing the bone cutting guide **20** across a targeted anatomy and/or positioning a bone or bones.

Additionally, the bone cutting guide **20** can have a secondary guide member **200**. The secondary guide member **200** can be supported on the rails **170A** and **170B**. For example, the secondary guide member **200** may include slots **205A** and **205B** to receive the rails **170A** and **170B** such that the secondary guide member **200** is supported thereon. The secondary guide member **200** can also have a third guide surface **210A** and a fourth guide surface **210B**. The third and fourth guide surfaces **210A** and **210B** can be adjacent surfaces facing one another with a space defined between the third and fourth guide surfaces **210A** and **210B**. In the illustrated embodiments, third and fourth guide surfaces **210A** and **210B** are single, continuous surfaces that do not include a gap, but in other embodiments third and/or fourth guide surfaces **210A** and **210B** can include a gap. The third guide surface **210A** defines a third plane, while the fourth guide surface **210B** defines a fourth plane. As shown, the third guide surface **210A** and fourth guide surface **210B** can be configured such that the third plane is parallel to the fourth plane, with the space between. In further embodiments (not illustrated), the guide surfaces **210A** and **210B** can be configured such that the third and/or fourth planes are skewed. Further, the third and/or fourth guide surfaces may be parallel to or skewed with respect to the first and/or second guide surfaces, such that the cutting guide can be adapted to make parallel cuts or angular cuts or cut shapes (e.g. a chevron shape). In some embodiments, the secondary guide member **200** can be locked to the rails **170A** and/or **170B** with a locking screw, cam, pin, etc. In the embodiment

shown in FIG. 3A, an aperture 214 is provided to receive a locking mechanism and/or an accessory, such as a handle.

FIGS. 4-6 illustrate perspective views of the embodiment of the bone cutting guide 20, described with respect to FIGS. 1-3, as assembled. In the embodiment illustrated in FIGS. 4-6, the bridge component 160 is attached to the main guide member 120 and both the fixating structure 180 and secondary guide member 200 are supported along the rails 170A and 170B of the bridge component. In one application, the secondary guide member 200 can be supported on the rails 170A and 170B at a location along the rails 170A and 170B between the fixating structure 180 and the main guide member 120. Additionally shown in FIGS. 4-6 are fixation pins 220A and 220B received within fixation apertures 190A and 190B such that the fixation pins 220A and 220B extend through the fixating structure 180. In some applications of the bone cutting guide 20, it may be desirable to provide the fixation pins 220A and 220B at an angle other than 90 degrees relative to a top surface of the fixating structure 180 by configuring the fixation apertures 190A and 190B to extend through the fixating structure 180 at a skewed angle to guide the fixation pins 220A and 220B. Fixation pins 220A and 220B can be used, for example, for stabilizing the bone cutting guide 20 across a targeted anatomy and/or positioning a bone or bones.

Embodiments of the bone cutting guide 20 can be useful in operation for temporarily positioning a bone or bones and guiding a cutting of a bone or bones at a targeted anatomy. Bone cutting can be useful, for instance, to facilitate contact between leading edges of adjacent bones, separated by a joint, or different portions of a single bone, separated by a fracture, such as in a bone alignment and/or fusion procedure. As such, embodiments of the present invention include methods for temporarily fixing an orientation of a bone or bones, such as during a surgical procedure, and guiding cutting at desired bone locations. In the embodiments described, cuts are made to bone with respect to the cutting guide, and the bones can be positioned for an additional surgical step, such as bone plating, after the cuts have been made.

FIGS. 7-16 illustrate steps of an embodiment of a method for temporarily positioning and cutting a bone or bones using the bone cutting guide 20. Specifically, FIGS. 7 and 8 show a perspective and top view, respectively, of the support 30 fixed to a bone 230 (e.g. a first metatarsal). The support 30 is placed on the bone 230. For embodiments of the bone cutting guide 20 that include the extensions 70A and 70B, the extensions 70A and 70B can be used to at least partially straddle the bone 230 and consequently provide both greater stability to the support 30 on the bone 230 and anatomical alignment of the support 30 on a longitudinal axis of the bone 230 (e.g., the slot 80 is generally parallel to the longitudinal axis of the bone 230). Extension member 72 can be adjusted to a desired distance from support 30. Further, in some embodiments it can be desirable to align and fix the support 30 along the longitudinal axis of the bone 230 using the fixation pins 60A and 60B. The pin 60A can be inserted through the fixation aperture 50A such that an end of the pin 60A protrudes out from the fixation aperture 50A adjacent the bone 230. The pin 60A can then be fixed to the bone 230. Similarly, the pin 60B can be inserted through fixation aperture 50B and fixed on an end to the bone 230. In this manner, the support 30 can be fixed in place to and aligned along the longitudinal axis of the bone 230.

In addition to fixing the support 30 to the bone 230, the main guide member 120 can be aligned such that the main guide member 120 is positioned at a location where a bone

(e.g., the bone 230) is to be cut. In one embodiment, the main guide member 120 can be positioned at the location where a bone is to be cut by appropriately positioning and fixing the support 30, e.g., such that the support 30 is fixed to the bone 230 at a location along bone 230 that results in the main guide member 120 being positioned at the location where a bone is to be cut. In some embodiments, a joint alignment blade (not shown) is inserted through the main guide member and into a joint space to help align the main guide member in a desired position. Further, in certain embodiments, a provisional fixation pin (not shown) can be inserted through a bone of interest and into an adjacent bone (e.g., through a first metatarsal and into a second metatarsal) to provide additional stability during the procedure.

In some applications, a location of the main guide member 120 relative to the longitudinal axis of the bone 230 can be adjusted without necessitating movement of the support 30. To accomplish this, the shaft 100 at least partially within the inner cavity 40 can be translated relative to the support 30 as shown in the perspective view of FIG. 9. As shown, the main guide member 120 has been translated along the longitudinal axis of the bone 230 a distance D as a result of the shaft 100 being moved the same distance D. Once the main guide member 120 is positioned at the location to be cut, the securing component 90 can be translated along the slot 80 such that the securing component 90 is aligned with securing aperture 110. The securing component 90 can then be fixed within the securing aperture 110 such that the shaft 100 is fixed relative to the support 30.

After the main guide member 120 has been positioned at the location to be cut, a cutting member (e.g. a saw blade) can be inserted through the space defined between the first guide surface 130A and the second guide surface 130B to cut, for example, the bone 230. The guide surfaces 130A and 130B can serve to direct the cutting member to the location of the bone 230 to be cut, which in many applications can be a precise location. The break or window defined in the second guide surface 130B can assist in visualizing the portion of the bone 230 being cut.

In some embodiments, the main guide member 120 can be used to make additional cuts. In such embodiments, the securing component 90 can be loosened and the shaft 100 can be translated within the cavity to a desired position. The securing component 90 can be then be fixed within the securing aperture so the shaft is again fixed relative to the support 30. In some embodiments, fixation pins may be inserted through fixation aperture 150A and/or 150B and into the bone 230 to further stabilize the main guide member. After the main guide member 120 has been repositioned at the location to be cut, a cutting member (e.g. a saw blade) can be inserted through the space defined between the first guide surface 130A and the second guide surface 130B to cut, for example, the bone 240. The guide surfaces 130A and 130B can serve to direct the cutting member to the location of the bone 240 to be cut.

In some applications, it may be desirable to provide additional, temporary fixation of the bone 230 to allow for more accurate cutting. As best seen again in FIG. 9, blocks 140A and 140B can provide a means for additionally positioning the bone 230. Fixation pins can be inserted through the fixation aperture 150A and/or 150B and into the bone 230 to temporarily position the bone 230 and/or adjacent bone 240 for cutting. In other applications, blocks 140A and 140B may not be necessary.

As shown in the perspective view of FIG. 10, once the bone 230 has been cut the bridge component 160 can optionally be attached to the main guide member 120. In one

embodiment, the bridge component **160** can have a geometry that allows the bridge component **160** to attach to the main guide member **120** between the first and second guide surfaces **130A** and **130B** through an interference fit, while in other embodiments the bridge component **160** can attach to the main guide member **120** by other attachment means. The rails **170A** and **170B** of the bridge component **160** can be arranged such that the rails **170A** and **170B** extend out from the bridge component **160** on a side of the bridge component **160** opposite the support **30**. The rails **170A** and **170B** can serve to support additional components of the bone cutting guide **20**.

One such component of the bone cutting guide **20** that can be supported on the rails **170A** and **170B** is the fixating structure **180**. FIG. **10** shows the fixating structure **180** attached to the rails **170A** and **170B**. In one embodiment, the fixating structure **180** can have holes or slots for receiving the rails **170A** and **170B** such that the fixating structure **180** can translate along the rails **170A** and **170B** to a desired position. The fixating structure **180**, for example, can also be secured to the rails **170A** and **170B** in a manner that prevents translation of the fixating structure **180** when desired by actuating the actuator **186**.

FIGS. **11** and **12** illustrate perspective views of the fixating structure **180** with the fixation pins **220A** and **220B** received through the fixation apertures **190A** and **190B** (**190B** is shown in, e.g., FIG. **2**). Fixation apertures **190A** and **190B** can be on opposite ends of the fixating structure **180** as shown. Fixation pins **220A** and **220B** can be fixed to a bone **240** (e.g. a first cuneiform as illustrated) to provide stability for the bone cutting guide **20** and/or to position the bone **240**. After the pins **220A** and **220B** are set, the fixating structure **180** can be translated with respect to the rails **170A** and **170B** and the support **30** to a desired position to compress or expand the space between the bones **230** and **240** as needed. The position of the bones can be locked by securing the fixating structure **180** against the rails **170A** and **170B**. In other embodiments, such compression or expansion can be achieved by moving the shaft **100** relative to the support **30** and reengaging the securing component **90** at the new desired position.

FIGS. **13** and **14** show perspective views of the bone cutting guide **20** assembled to include the secondary guide member **200**. The secondary guide member **200** can be supported on the rails **170A** and **170B**. In one embodiment, the slots **205A** and **205B** of the secondary guide member **200** can receive the rails **170A** and **170B** such that the secondary guide member **200** can translate along the rails **170A** and **170B** to a desired position. As illustrated, the secondary guide member **200** can be located along the rails **170A** and **170B** between the fixating structure **180** and the bridge component **160**.

The secondary guide member **200** can be positioned at a location where a second bone cut is to be made. A cutting member (e.g. a saw blade) can be inserted through the space defined between the third and fourth guide surfaces **210A** and **210B** to cut, for example, the bone **240**. The guide surfaces **210A** and **210B** can serve to direct the cutting member to the location of the bone **240** to be cut, which in many applications can be a precise location. As illustrated, the cut made using the secondary guide member **200** (e.g. to bone **240**) will be a cut that is generally parallel to the cut made using the main guide member **120**. However, in other embodiments components of the bone cutting guide **20** (e.g. rails **170A** and **170B**) can be configured such that the cut

made using the secondary guide member **200** is an angular cut (i.e. not parallel) relative to the cut made using the main guide member **120**.

FIGS. **15** and **16** illustrate the bone cutting guide **20** as described previously, with the secondary guide member **200** translated along the rails **170A** and **170B**. The secondary guide member **200** can be translated along the rails **170A** and **170B** to precisely locate the secondary guide member **200** at the location to be cut (e.g. on bone **240**). In the embodiment illustrated, the secondary guide member **200** can be shaped such that a portion of the secondary guide member **200** can overlap, or sit on top of, the bridge component **160**. Such a configuration can be useful, for example, where the second cut made using the secondary guide member **200** is desired to be close to the first cut made using the main guide member **120** (e.g. portions of bones **230** and **240** interfacing at a joint).

When the bone **230** and/or bone **240** have been cut and positioned as desired, the bone cutting guide **20** can be removed. In some embodiments, the cutting guide **20** is temporarily removed from the fixation pins and cut bone is removed from the area. In certain embodiments, an autograft or other compound is delivered to the area of the bone cuts. Optionally, the guide may then be reset on the bones over the fixation pins and the shaft **100** can be translated within the cavity to adjust the relative position of the bones (e.g., to compress them together). The securing component **90** can be then be fixed within the securing aperture so the shaft is again fixed relative to the support **30**. A bone plate may optionally be applied across the joint while the bones are held in the longitudinally fixed position by the cutting guide. After the plate is applied, the bone cutting guide and the fixation pins may be removed. Removing the bone cutting guide **20** can include removing all fixation pins and the support, and, in some embodiments, can include removing the bridge component, along with the fixation structure and secondary guide member **200**. In certain embodiments, a second bone plate may optionally be applied across the joint. In a specific embodiment, the two bone plates are applied about 90 degrees from each other around the circumferences of the bones (e.g., at a dorsal side and a medial side).

Thus, embodiments of the invention are disclosed. Although the present invention has been described with reference to certain disclosed embodiments, the disclosed embodiments are presented for purposes of illustration, and not limitation, and other embodiments of the invention are possible. One skilled in the art will appreciate that various changes, adaptations, and modifications may be made without departing from the spirit of the invention.

The invention claimed is:

1. A method of correcting an alignment between bones of a foot, the method comprising:
 - positioning a first cutting slot of a bone cutting guide over a metatarsal;
 - inserting a cutting member through the first cutting slot to remove a portion of the metatarsal;
 - adjusting an alignment of the metatarsal relative to a cuneiform separated from the metatarsal by a joint to establish a moved position of the metatarsal;
 - positioning a second cutting slot of the bone cutting guide over the cuneiform;
 - inserting the cutting member through the second cutting slot to remove a portion of the cuneiform; and
 - causing the metatarsal to fuse to the cuneiform in the moved position.
2. The method of claim 1, wherein the bone cutting guide comprises a fixation aperture positioned distally of the first

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cutting slot, and further comprising inserting a fixation pin through the fixation aperture and into the metatarsal prior to inserting the cutting member through the first cutting slot.

3. The method of claim 1, wherein the bone cutting guide comprises a fixation aperture positioned proximally of the second cutting slot, and further comprising inserting a fixation pin through the fixation aperture and into the cuneiform prior to inserting the cutting member through the second cutting slot.

4. The method of claim 1, wherein the second cutting slot is parallel to the first cutting slot, such that inserting the cutting member through the first cutting slot and inserting the cutting member through the second cutting slot results in a cut end of the metatarsal being parallel to a cut end of the cuneiform.

5. The method of claim 1, wherein the second cutting slot is angled relative to the first cutting slot, such that inserting the cutting member through the first cutting slot and inserting the cutting member through the second cutting slot results in a cut end of the metatarsal being angled relative to a cut end of the cuneiform.

6. The method of claim 1, wherein the cutting member is a saw blade.

7. The method of claim 1, wherein positioning the first cutting slot over the metatarsal comprises positioning an alignment window defined by the bone cutting guide over the joint.

8. The method of claim 1, further comprising inserting a joint alignment blade through the bone cutting guide and into the joint to align the bone cutting guide.

9. The method of claim 1, wherein inserting the cutting member through the first cutting slot and inserting the cutting member through the second cutting slot comprises inserting the cutting member through the first cutting slot to remove the portion of the metatarsal prior to inserting the cutting member through the second cutting slot to remove the portion of the cuneiform.

10. The method of claim 1, wherein inserting the cutting member through the first cutting slot and inserting the cutting member through the second cutting slot comprises inserting the cutting member through the first cutting slot to remove the portion of the metatarsal after inserting the cutting member through the second cutting slot to remove the portion of the cuneiform.

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11. The method of claim 1, wherein the bone cutting guide comprises:

a first guide surface defining a first plane and a second guide surface defining a second plane, with the first cutting slot being provided between the first plane and the second plane, and

a third guide surface defining a third plane and a fourth guide surface defining a fourth plane, with the second cutting slot being provided between the third plane and the fourth plane.

12. The method of claim 1, wherein positioning the first cutting slot over the metatarsal and positioning the second cutting slot over the cuneiform comprises positioning the bone cutting guide on a dorsal side of the metatarsal and the cuneiform.

13. The method of claim 1, wherein causing the metatarsal to fuse to the cuneiform in the moved position comprises delivering a compound to an area between a cut end of the metatarsal and a cut end of the cuneiform.

14. The method of claim 1, wherein causing the metatarsal to fuse to the cuneiform in the moved position comprises applying a bone plate across the joint.

15. The method of claim 14, wherein applying the bone plate comprises applying the bone plate while the metatarsal and cuneiform are held in the moved position by the bone cutting guide.

16. The method of claim 14, wherein the bone plate comprises a first bone plate, and further comprising applying a second bone plate across the joint.

17. The method of claim 16, wherein applying the first bone plate comprises applying the first bone plate on a dorsal side of the metatarsal and cuneiform, and applying the second bone plate comprises applying the second bone plate on a medial side of the metatarsal and cuneiform.

18. The method of claim 1, further comprising translating the second cutting slot perpendicularly relative to the first cutting slot to adjust a separation distance between the first cutting slot and the second cutting slot.

19. The method of claim 1, wherein causing the metatarsal to fuse to the cuneiform in the moved position comprises compressing the metatarsal and the cuneiform together.

20. The method of claim 1, wherein the metatarsal is a first metatarsal and the cuneiform is a first cuneiform.

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